



Effects of Isometric Exercise on Muscle Activity and Body Balance Ability in Asymmetrical Walkers*

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Abstract

Purpose: This study was to investigate the effects of isometric exercise on muscle activity and body balance ability in asymmetrical walkers. **Research design, data, and methodology:** Twenty gait asymmetry people were divided to unilateral exercise group (UG, n=10) and bilateral exercise group (BG, n=10). UG were performed unilateral exercise for 60 minutes, three times a week, and 16 weeks, and BG were performed one side and then the other side alternately for 60 minutes, three times a week, and 16 weeks. Muscle activity and body balance ability were measured before, after 4 and 16 weeks isometric exercise. Moreover, SI (symmetry index; SI) was calculated from the measured value of SL (step length). Statistical analyses were conducted using one-way ANOVA and two-way ANOVA with repeated measures, a paired t-test, and multiple comparisons according to Scheffe. **Results:** In the muscle activity, ST decreased significantly in short step length(S-SL) and BG of LS compared to before isometric exercise($p<.05$), and GCM decreased significantly in BG of S-SL($p<.05$). As for body balance ability, the mSEBT-A difference between L-SL and S-SL was decreased significantly in UG($p<.05$). And the respective total scores of L-SL and S-SL, mSEBT-PM and mSEBT-PL were increased significantly in BG($p<.05$). **Conclusions:** As a result, in this study above, it was confirmed that isometric exercise improved muscle activity and body balance ability in asymmetrical walkers.

Keywords: Isometric Exercise, Muscle Activity, Body Balance Ability, Asymmetrical Walker

JEL Classification Code: I10, I12, I18

1. Introduction

According to the "Life Table" data from the Korean Statistical Office in 2021, the average life expectancy for Koreans in 2020 was 80.5 years for men and 86.5 years for women, with an overall average of 83.5 years. According to the World Health Organization's health statistics for 2020, the healthy life expectancy of Koreans, measured by prevention and management rather than disease treatment, was 73.1 years for both genders. The average age for Korean women experiencing menopause, which can lead to rapid changes in health due to hormonal fluctuations, was 49.3 years. The concept of healthcare is shifting from simply extending life expectancy through disease treatment to extending healthy life expectancy through prevention and management. In terms of exercise science, research has provided significant evidence for preventing degenerative diseases and lifestyle-related illnesses, as well as increasing quality of life and healthy aging. Furthermore, physical inactivity has become a significant risk factor for various diseases, including COVID-19, in addition to aging and transplant

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history. As a major guideline for disease prevention, exercise habits are recommended in the field of public health (Varela et al., 2021; Park, 2021). As medical technology advances, many patients are experiencing discomfort in walking, which is the ultimate goal of rehabilitation programs due to a decrease in physical function, including balance, strength, walking speed, and stroke caused by aging-related diseases after their 60s (Perry & Burnfield, 2010; Sharma & Kaur, 2017). Therefore, in addition to positive results, there are many aspects to consider regarding abnormal results in research to improve walking, the most common activity among all human activities (Sadeghi et al., 2000). Herzog et al. (1989) quantified the symmetry and asymmetry of walking in healthy people using the Symmetry Index (SI) and considered a range of asymmetrical walking between 4% and 13% as a threshold for abnormal walking. Mills (1994) focused on symmetry improvement, observing low levels of asymmetry in the early stages of disease and high levels of asymmetry in the later stages. Studies conducted with a focus on unilateral exercise, considering asymmetry, include research comparing the effects of unilateral exercise that considers lower limb muscle asymmetry and bilateral exercise that does not consider lower limb asymmetry. Other studies have investigated the effects of unilateral exercise on balance and temporal gait variables in stroke patients, demonstrating significant functional improvements in static, dynamic, and functional balance abilities and temporal gait variables. Additionally, research has been conducted on unilateral exercise for bowling players who are prone to easy left-right asymmetry, providing an appropriate stretching training program to improve body misalignment symptoms and correct incorrect posture to prevent injury (Kim et al., 2014; Park, 2014). Furthermore, research on isokinetic exercise aimed at reducing asymmetry by applying exercise unilaterally is currently underway, but further research is needed as the evidence is not yet sufficient (Bishop et al., 2021; Gonzalo-Skok et al., 2015; Núñez et al., 2018; Bishop et al., 2018).

2. Methods

2.1 Subject

The subjects were selected from members registered at the G center in K region who had no orthopedic surgery or deformity, no neurological damage, and had a symmetry index (SI) of 4-13% in one-step length during walking, which indicates asymmetric gait (Zifchock et al., 2008). The SI was calculated using the formula presented by Robinson et al. (1987) to determine the asymmetry index of walking. Using G-Power 3.1.9.7, a sample size of eight subjects was required, assuming an effect size of .50, a significance level of .05, and a power of .80, accounting for potential dropouts. Thus, 20 subjects were recruited, with 10 participants in the unilateral exercise group (UG) and 10 in the bilateral exercise group (BG). Participants were briefed on the purpose and experimental procedures of the study and only those who had no issues with the PAR-Q Test were included. The physical characteristics of the study participants are shown in <Table 1>. This study was approved by the Institutional Review Board of E University (EU22-56).

Table 1: Physical characteristics of subjects

Group(n)	Age (years)	Weight (kg)	Height (cm)	SMM (kg)	Leg length (cm)	SI (%)
UG(10)	48.1±3.38	64.17±8.80	157.48±4.46	21.01±2.09	80.60±3.57	5.04±0.65
BG(10)	48.8±3.11	57.34±9.17	160.73±4.22	22.22±1.96	80.10±2.26	4.75±0.86

means ± SD.

2.2 Interventions

The exercise program was conducted for 16 weeks, 3 times per week, for 60 minutes each session, with feedback provided by experienced instructors in a 1:1 setting. The specific exercise regimen consisted of six weight-bearing exercises (calf raise hold, split squat, resisted knee flexion, prone leg lift, single leg deadlift, single leg bridge) targeting the muscle groups activated during walking, preceded by a 10-minute warm-up on a treadmill and followed by a 10-minute cool-down on the same treadmill (Tsaklis et al., 2015; Perry & Burnfield, 2010). The exercise protocol was divided into two groups: the unilateral exercise group (UG) and the bilateral exercise group (BG). The UG group performed each exercise for 30 seconds, 5 sets per session, with a 30-second rest between sets and a 120-second rest between exercises, for a total of 40 minutes per session<Table 2>. The UG group selected the longer stride length side between the left and right sides for each exercise. The BG group alternated

between left and right sides for each exercise, following the same protocol as the UG group. The intensity of all exercises was set at a subjective intensity level of RPE 11-13 (11-easy, 12-moderate, 13-slightly difficult), and the exercise intensity was adjusted by increasing the angle range of each exercise based on RPE measurements every four weeks.

Table 2: Exercise program

Order	Type	Intensity	Time	Frequency
Warm-up	treadmill walking	RPE 11~13	10 min	
Main exercise	calf raise hold	30 sec	40 min	3 times / w
	split squat	30 sec		
	Resisted knee flexion	30 sec		
	prone leg lift	30 sec		
	single leg deadlift	30 sec		
	single leg bridge	30 sec		
Cool-down	treadmill walking	RPE 11~13	10 min	
Note	When performing sets in the BG group, perform one side and then the other side alternately.			

2.3 Metrics

2.2.1 Muscle Activity

Muscle activation was measured using wireless electromyography equipment (mini DTS, Noraxon Inc., USA) before exercise, 4 weeks, 8 weeks, 12 weeks, and 16 weeks after exercise. Electrode attachment sites recommended in the electromyography manual were used, which are important for diagnosing cerebral palsy and sports injuries in athletes, and for affecting energy consumption during walking in elderly people. The measurement was conducted on the semitendinosus muscle of the thigh, which has a significantly high amplitude during walking, and the medial gastrocnemius muscle, which increases stability during the stance phase of walking, among the calf muscles (Konrad, 2005; Blitz & Eliot, 2007; Aquino et al., 2010; Jang, 2010). The skin was shaved with a razor to minimize skin resistance, and alcohol was used to disinfect and remove measurement errors. EMG wet gel electrodes (Single electrode T246H, SEED TECH, KOREA) were used to attach the electrodes to the muscle belly. The muscle impedance was kept below 70K ohms, and the sampling rate was set at 1,500 Hz with a frequency bandwidth of 20-500 Hz to filter out noise. The collected data were analyzed using Noraxon MR3 3.14 software. For each muscle, the maximal voluntary isometric contraction (MVIC) was performed three times for five seconds each time (Kendall et al., 2005), and the electromyography signal was collected from the first left initial contact to four strides using GAITrite, which allowed for natural walking. The muscle activation data were quantified as the root mean square (RMS) value and standardized as a percentage of MVIC (%MVIC) during walking.

2.2.2 Body Balance Ability

The study used the Modified Star Excursion Balance Test (mSEBT) with a high reliability of 0.89-0.94 for evaluating dynamic balance to measure the physical balance ability before exercise and at 4, 8, 12, and 16 weeks after exercise (Gribble et al., 2013; Fullam et al., 2014). The mSEBT evaluates balance ability by finding and evaluating the minimum overlapping information of the 8 directions with a 45° interval in the Star Excursion Balance Test (SEBT), which includes the anterior (SEBT-A), anterior-medial (SEBT-AM), medial (SEBT-M), posterior-medial (SEBT-PM), posterior (SEBT-P), posterior-lateral (SEBT-PL), lateral (SEBT-L), and anterior-lateral (SEBT-AL) directions. The evaluation was simplified by using only three directions, the anterior (ANT), posterior-medial (PM), and posterior-lateral (PL), which could be easily used for management (Hertel et al., 2006). The study drew lines and had participants stand on one leg in the center while reaching out with the other leg as far as possible along each direction's line. The distance from the tip of the toe of the extended leg to the center was measured in cm. Limb length (LL) was measured from the anterior superior iliac spine to the most superior point

of the medial malleolus while lying down, and data for each direction were calculated. The participants were given an explanation of the measurement procedure and a demonstration before measuring the average of three repetitions (Bulow et al., 2019). If the extended foot did not touch the ground, the supporting foot lost contact with the ground, or the starting position could not be returned to after extending the foot, it was considered a failure, and the measurement was repeated. Both left and right sides underwent mSEBT.

3. Results

3.1 Muscle Activity

The changes in muscle activity of the unilateral exercise group and bilateral exercise group over 16 weeks are presented in <Table 3>. The results of the two-way repeated measures ANOVA for muscle activity of the ST and GCM showed significant differences in ST in the BG of S-SL at 4 weeks ($p=0.030$), 8 weeks ($p=0.016$), 12 weeks ($p=0.007$), and 16 weeks ($p=0.018$) compared to before exercise, and there was no significant interaction between group and time ($F=5.253$, $p<0.001$). In addition, there were significant differences in L-SL's BG at 4 weeks ($p=0.002$), 8 weeks ($p=0.000$), 12 weeks ($p=0.000$), and 16 weeks ($p=0.000$) compared to before exercise, and there was a significant interaction between group and time at 8 weeks ($p=0.004$), 12 weeks ($p=0.000$), and 16 weeks ($p=0.000$) ($F=8.123$, $p<0.001$), but there was no significant difference between groups. GCM showed significant differences in S-SL's BG at 4 weeks ($p=0.009$), 8 weeks ($p=0.010$), 12 weeks ($p=0.030$), and 16 weeks ($p=0.020$) compared to before exercise ($F=2.526$, $p<0.05$), and there was no significant interaction between group and time. On the other hand, there were no significant differences in group, time, or interaction between group and time for L-SL.

Table 3: Changes in muscle activity in two groups for 16 weeks

	group (n=10)	before	4-wk	8-wk	12-wk	16-wk	$\Delta\%$	repeated measure		
								F-value	P-value	
ST (%)	UG	94.69	85.41	81.39	82.09	80.00	-15.51	G	0.339	0.562
		± 22.63	± 13.20	± 15.51	± 12.89	± 12.62		T	5.253	0.001**
	S-SL BG	108.24	75.73	76.86	72.51	78.80	-27.20	GxT	1.181	0.325
		$\pm 32.96^a$	$\pm 19.20^b$	$\pm 17.69^b$	$\pm 15.71^b$	$\pm 14.39^b$				
		t-value	1.017	-1.246	-0.578	-1.414	-0.188			
		p-value	0.324	0.231	0.572	0.176	0.853			
L-SL	UG	96.00	87.86	79.97	83.63	80.49	-16.16	G	0.764	0.385
		± 22.91	± 12.57	± 16.62	± 12.30	± 10.96		T	8.123	0.000***
	BG	126.20	90.49	84.72	71.92	73.86	-41.47	GxT	2.704	0.036*
		$\pm 46.66^a$	$\pm 18.38^b$	$\pm 11.50^b$	$\pm 18.43^b$	$\pm 12.04^b$				
		t-value	1.743	0.354	0.706	-1.586	-1.221			
		p-value	0.101	0.728	0.491	0.132	0.240			
GCM S-SL	UG	93.29	76.05	76.23	81.06	81.89	-12.22	G	1.396	0.241

(%)		±41.66	±24.93	±24.96	±18.04	±22.93			
							T	2.526	0.047*
	BG	94.43	70.85	71.83	73.12	70.01			
		±19.17 ^a	±18.54 ^b	±7.60 ^b	±19.04 ^b	±13.76 ^b	-25.86		
							G×T	0.201	0.937
	<i>t</i> -value	0.075	-0.502	-0.506	-0.908	-1.332			
	<i>p</i> -value	0.941	0.623	0.620	0.377	0.201			
							G	0.015	0.904
	UG	93.29	82.48	75.48	74.29	74.70			
		±41.66	±15.83	±23.99	±18.42	±39.97	-19.93		
							T	1.182	0.325
L-SL	BG	85.39	83.99	79.82	72.98	74.80			
		±14.41	±14.49	±28.82	±21.76	±16.87	-12.40		
							G×T	0.144	0.965
	<i>t</i> -value	-0.537	0.211	0.347	-0.137	0.007			
	<i>p</i> -value	0.598	0.835	0.733	0.893	0.995			

means ± SD. * $p < .05$. ** $p < .01$. *** $p < .001$.

^{a,b,c,d}Significantly different from before ($p < .05$).

ST; Semitendinosus. GCM; Gastrocnemius Muscle.

S-SL; Short Step Length. L-SL; Long Step Length.

UG; Unilateral exercise Group. BG; Bilateral exercise Group.

3.2 Body Balance Ability

3.2.1 DB and TS

The changes in the balance abilities of DB and TS in the unilateral exercise group and bilateral exercise group over 16 weeks are presented in <Table 4>. The two-way mixed-design ANOVA for mSEBT of DB and TS showed that there was a significant difference between groups for DB in the UG ($F=4.268$, $p<.05$), but no significant interaction effect between time and group or time alone. For TS, there was a significant difference between groups for both S-SL and L-SL in BG ($F=4.756$, $p<.05$; $F=8.563$, $p<.05$), but no significant interaction effect between time and group or time alone.

Table 4: Changes in dynamic balance ability in two groups for 16 weeks

	group (n=10)	before	4-wk	8-wk	12-wk	16-wk	$\Delta\%$	repeated measure ANOVA		
								<i>F</i> -value	<i>P</i> -value	
DB (cm)	UG	6.35	4.12	4.50	4.06	3.68	-42.05	G	4.268	0.042*
		±2.56	±3.06	±2.79	±3.10	±1.31		T	0.406	0.804
	BG	5.91	6.64	5.38	6.08	6.10	3.21	G×T 0.613		0.654
		±2.97	±5.17	±3.01	±4.86	±3.48				
	<i>t</i> -value	0.335	-1.255	-0.642	-1.049	-1.957				
	<i>p</i> -value	0.742	0.227	0.530	0.310	0.068				
TS (score)	S-SL UG	7.82	7.18	7.24	7.64	7.98	2.05	G	8.563	0.004*
		±0.56	±0.78	±0.82	±0.81	±0.94		T	0.864	0.489

	BG	7.69 ±1.29	7.98 ±1.23	8.17 ±1.28	8.10 ±1.01	8.17 ±0.75	6.24		
	<i>t</i> -value	0.064	-1.919	-1.915	-1.323	-1.418		G×T 0.610	0.656
	<i>p</i> -value	0.950	0.073	0.074	0.204	0.175			
	UG	7.43 ±1.21	7.03 ±1.00	7.01 ±1.02	7.41 ±1.12	7.67 ±1.28	3.23	G 4.756 T 0.673	0.032* 0.612
L-SL	BG	7.47 ±1.11	7.94 ±1.03	8.09 ±1.34	8.01 ±0.73	8.39 ±0.84	12.32	G×T 0.891	0.474
	<i>t</i> -value	0.284	-1.635	-1.838	-1.062	-0.483			
	<i>p</i> -value	0.950	0.122	0.085	0.304	0.636			

means ± SD. * *p* < .05.

DB; Discrepancy Between Long-Short

TS; Total Score

S-SL; Short Step Length. L-SL; Long Step Length.

UG; Unilateral exercise Group. BG; Bilateral exercise Group.

3.2.2 mSEBT-PM, mSEBT-PL, and mSEBT-A

The changes in mSEBT-PM, mSEBT-PL, and mSEBT-A of the unilateral exercise group and the bilateral exercise group's physical balance abilities over 16 weeks are presented in <Table 5>. The two-way mixed-design ANOVA for mSEBT-PM, mSEBT-PL, and mSEBT-A showed that mSEBT-PM significantly differed between groups in S-SL and L-SL in BG(*F*=6.903, *p*<0.05; *F*=6.560, *p*<0.05), but no significant interaction was found between time, group, and time, and no significant difference was found for mSEBT-PL in time, group, and time interaction. Moreover, mSEBT-A did not show any significant difference in group, time, and group and time interaction after exercise compared to before exercise.

Table 5: Changes in dynamic balance ability in two groups 16 weeks

	group (n=10)	before	4-wk	8-wk	12-wk	16-wk	Δ%	repeated measure ANOVA	
								<i>F</i> -value	<i>P</i> -value
mSEBT -PM (%)	UG	77.31 ±9.53	69.22 ±12.14	68.53 ±11.93	75.83 ±14.02	78.89 ±14.12	2.04	G	6.903 0.010*
								T	0.366 0.832
	S-SL BG	78.59 ±24.09	83.14 ±24.95	83.94 ±13.38	86.12 ±14.48	81.91 ±12.10	4.22	G×T	0.724 0.578
		<i>t</i> -value	-0.148	-1.505	-2.578	-1.531		-0.488	
		<i>p</i> -value	0.884	0.152	0.020*	0.145	0.632		
	L-SL UG	70.19 ±23.56	66.26 ±15.86	66.59 ±17.78	70.36 ±21.08	75.35 ±24.97	7.35	G	6.560 0.012*
						T		0.758 0.556	

	BG	73.14 ±14.02	78.80 ±10.57	79.08 ±19.65	79.11 ±8.72	85.74 ±9.25	17.23	G×T	0.231 0.920
	<i>t</i> -value	-0.322	-1.974	-1.415	-1.151	-1.170			
	<i>p</i> -value	0.752	0.066	0.176	0.267	0.259			
	UG	92.61 ±5.82	83.10 ±7.62	85.60 ±8.24	89.49 ±11.95	94.78 ±13.43	2.34	G	3.993 0.049*
								T	1.231 0.304
	S-SL BG	89.87 ±11.11	92.72 ±11.59	96.20 ±19.31	93.91 ±14.60	98.98 ±14.52	10.14	G×T	0.830 0.510
	<i>t</i> -value	0.656	-0.082	-1.515	-0.703	-0.638			
	<i>p</i> -value	0.521	0.054	0.149	0.492	0.532			
mSEBT -PL (%)	UG	88.93 ±13.33	81.25 ±11.70	80.98 ±11.46	87.88 ±12.42	89.92 ±15.52	1.11	G	16.004 0.000***
								T	0.800 0.529
	L-SL BG	91.25 ±15.24	96.69 ±14.59	98.19 ±17.15	97.88 ±8.05	101.60 ±12.64	11.34	G×T	0.838 0.505
	<i>t</i> -value	-0.344	-2.476	-2.503	-2.028	-1.751			
	<i>p</i> -value	0.736	0.025+	0.024+	0.060	0.099			
	UG	90.73 ±11.32	87.14 ±10.53	87.07 ±10.75	88.55 ±9.66	92.34 ±8.08	1.77	G	0.252 0.617
								T	0.260 0.903
	S-SL BG	87.76 ±13.60	90.00 ±11.36	92.10 ±14.45	90.10 ±7.75	91.57 ±8.08	4.34	G×T	0.377 0.825
	<i>t</i> -value	0.504	-0.555	-0.839	-0.376	0.203			
	<i>p</i> -value	0.621	0.587	0.414	0.712	0.842			
mSEBT -A (%)	UG	88.57 ±10.34	86.73 ±10.62	86.13 ±10.39	88.92 ±8.78	90.32 ±8.67	1.98	G	0.443 0.507
								T	0.442 0.778
	L-SL BG	84.48 ±11.58	89.30 ±13.05	92.69 ±12.85	89.88 ±14.05	92.36 ±12.68	9.33	G×T	0.503 0.733
	<i>t</i> -value	0.791	-0.458	-1.190	-0.174	-0.398			
	<i>p</i> -value	0.440	0.653	0.251	0.864	0.696			

means ± SD. * $p < .05$. *** $p < .001$. + $p < .05$ vs between groups within time.

mSEBT; modified star excursion balance test. PM; posterior-medial, PL; posterior-lateral. A; anterior.

S-SL; Short Step Length. L-SL; Long Step Length.

UG; Unilateral exercise Group. BG; Bilateral exercise Group.

4. Discussion

In this study, we designed an exercise program to increase balance and stability during walking by promoting complementary development of the muscles around the hip joint, knee joint, glutes, and spinal erectors. We compared a unilateral exercise group that performed stability exercises on one side and a bilateral exercise group that performed alternating stability exercises on both sides to analyze the changes in muscle activity of the tensor fasciae latae and adductor muscles, which greatly affect the early-midstance and late stance phases of the gait cycle.

The results showed that the %MVIC of the tensor fasciae latae decreased in both exercise groups, and the %MVIC of the adductor muscles on the shorter step side significantly decreased in both exercise groups. Calf raised hold exercise involves the tibialis anterior muscle, which reduces the time the front foot touches the ground during walking, leading to an increase in initial contact time. This is consistent with previous studies showing that an increase in initial contact time leads to increased muscle activation of the quadriceps, hamstrings, and tibialis anterior muscles (Khallaf et al., 2014; Sutherland, 2001). Split squat exercise improves muscle control of hip adduction during the stance phase of the gait cycle, enhancing stability (McCurdy, 2017), while resisted knee flexion exercise increases muscle activation of the adductor muscles of the inner thigh by rotating the knee joint inward (Yanagisawa & Fukutani, 2020). Prone leg lift exercise activates the spinal erectors, glutes, and hamstrings (Sakamoto & Teixeira-Salmela, 2009), and single-leg deadlift exercise activates the erector spinae muscles (Shaikh & Moharkar, 2020). Single-leg bridge exercise minimizes excessive use of the spinal erectors and acts as an important factor in reducing knee joint pain during walking or hill climbing by affecting knee joint angle (Pori et al., 2021). The increase in muscle activation of the tensor fasciae latae, which is responsible for hip abduction and knee flexion, observed in this study supports the results of Hublely-Kozey et al.'s (2009) study, which showed a higher amplitude of activation in the tensor fasciae latae than in the adductor muscles during walking. It also aligns with previous research showing significant changes in muscle activation after six weeks of exercise targeting the hamstrings in healthy adults. Therefore, this study confirms that a 16-week stability exercise program can positively affect muscle activation in middle-aged women.

In this study, the modified Star Excursion Balance Test (mSEBT) was used to measure the balance ability of a unilaterally-trained group that performed unilateral exercises for the contralateral side and a bilaterally-trained group that performed alternating unilateral exercises for both sides. The mSEBT-A was measured to compare the difference between the two sides, and the total scores of the left and right sides, mSEBT-A, mSEBT-PM, and mSBBT-PL were analyzed. The results showed that the difference between the two sides in mSEBT-A decreased in the unilaterally-trained group, and the total scores of the short step side and the long step side increased in the bilaterally-trained group. In addition, the reaching distance of mSEBT-PM and mSBBT-PL also improved in the bilaterally-trained group. These results are consistent with previous studies that reported enhanced leg strength, flexibility, and proprioceptive sensation after balance ability exercises in middle school volleyball players and increased total scores in the left and right sides after exercise in elementary school soccer players. Furthermore, it is suggested that the balance stability to maintain body balance is improved by controlling the bilateral muscle strength imbalance. Therefore, in this study, a 16-week balance exercise program was found to be effective in reducing the difference between the two sides by applying unilateral exercises and increasing balance ability by applying bilateral exercises, which could have a positive impact on the balance ability of middle-aged women and could serve as evidence for preventing fall accidents in the elderly caused by a decline in balance ability.

References

- Aquino, C. F., Fonseca, S. T., Goncalves, G. G., Silva, P. L., Ocarino, J. M., & Mancini, M. C. (2010). Stretching versus strength training in lengthened position in subjects with tight hamstring muscles: a randomized controlled trial. *Manual Therapy, 15*(1), 26-31.
- Bishop, C., Turner, A., & Read, P. (2018). Training methods and considerations for practitioners to reduce interlimb asymmetries. *Strength & Conditioning Journal, 40*(2), 40-46.
- Bishop, C., Read, P., Lake, J., Loturco, I., Dawes, J., Madruga, M., Romero-Rodrigues, D., Chavda, S., & Turner, A. (2021). Unilateral isometric squat: Test reliability, interlimb asymmetries, and relationships with limb dominance. *Journal of Strength and Conditioning Research, 35*, 144-151.
- Blitz, N. M., & Eliot, D. J. (2007). Anatomical aspects of the gastrocnemius aponeurosis and its insertion a cadaveric study. *Journal of Foot and Ankle Surgery, 46*(2), 101-108.
- Bulow, A., Anderson, J. E., Leiter, J. R., MacDonald, P. B., & Peeler, J. (2019). The modified star excursion balance and Y-balance test results differ when assessing physically active healthy adolescent females. *International journal of sports Physical Therapy, 14*(2), 192-203.
- Fullam, K., Caulfield, B., Coughlan, G. F., & Delahunt, E. (2014). Kinematic analysis of selected reach directions of the Star Excursion Balance Test compared with the Y-Balance Test. *Journal of sport rehabilitation, 23*, 27-35.
- Gonzalo-Skok, O., Tous-Fajardo, J., Suarez-Arrones, L., Arjol-Serrano, J. L., Casajús, J. A., & Mendez-Villanueva, A. (2015). Single-leg power output and between-limbs imbalances in team-sport players: Unilateral versus bilateral combined resistance training. *Journal of Sports Physiology and Performance, 12*(1), 106-114.
- Gribble, P. A., Kelly, S. E., Refshauge, K. M., & Hiller, C. E. (2013). Interrater reliability of the star excursion balance test. *Journal of athletic training, 48*(5), 621-626.
- Hertel, J., Braham, R. A., Hale, S. A., & Olmsted-Kramer, L. C. (2006). Simplifying the star excursion balance test: analyses of subjects with and without chronic ankle instability. *Journal Orthopedic Sports Physical Therapy, 36*(3), 131-137.
- Herzog, W., Nigg, B. M., Read, L. J., & Olsson, E. (1989). Asymmetries in ground reaction force patterns in normal human gait. *Medicine and Science in Sports and Exercise, 1*, 110-114.

- Hubley-Kozey, C. L., Hill, N. A., Rutherford, D. J., Dunbar, M. J., & Stanish, W. D. (2009). Co-activation differences in lower limb muscles between asymptomatic controls and those with varying degrees of knee osteoarthritis during walking. *Clinical Biomechanics*, 24(5), 407-414.
- Jang, E. H., Chi, S. Y., Lee, J. Y., Cho, Y. J., Chun, B. T., (2010). Gait phases detection from EMG and FSR signals in walking. *Science of emotion & sensibility*, 13(1), 207-214.
- Kang, Y. H., & KiM, C. S., (2021). Functional movement evaluation, body balance, vital capacity effects after a 10-week body stabilization program for elementary school. *Journal of the korea academia industrial cooperation society*, 22(7), 40-50.
- Kendall, F. P., McCreary, E. K., Provance, P. G., Rodgers, M. M., & Romani, W. A. (2005). *Muscles: Testing and Function with Posture and Pain*, 5th edition. Baltimore. *Lippincott Williams & Wilkins*, 410-421.
- Khallaf, M. E., Gabr, A. M., & Fayed, E. E. (2014). Effect of task specific exercises, gait training, and visual biofeedback on equinovarus gait among individuals with stroke: Randomized controlled study. *Neurology research international*, e693048.
- Kim, D. W., Hwang, B. Y., & Jung, S. M. (2014). The effects of applying alignment control to unilateral stepping exercise training on improving balance and ability in post stroke hemiplegia. *The journal of Korean society for neurotherapy*, 18(1), 1-6.
- Konrad, P. (2005). *The ABC of EMG: A practical introduction to kinesiological electromyography*. Noraxon Inc. USA. 19-20.
- McCurdy, K. (2017). Technique, variation, and progression of the rear-foot-elevated split squat. *Strength and Conditioning Journal*, 9(6), 93-97.
- Mills, E. M. (1994). The effect of low-intensity aerobic exercise on muscle strength, flexibility and balance among sedentary elderly persons. *Nursing Research*, 43(4), 207-211.
- Núñez, F. J., Santalla, A., Carrasquilla, L., Asian, J. A., Reina, J. L., & Suar ez-Arrones, L. J. (2018). The effects of unilateral and bilateral eccentric overload training on hypertrophy, muscle power and COD performance, and its determinants, in team sport players. *PLoS ONE*, 13(3), e0193841.
- Park, H. T. (2021). The role of exercise science in hypokinetic society. *Korean society of exercise physiology*, 30(3), 273-277.
- Park, S. T. (2014). Effect of unilateral and bilateral resistance training on muscle force, power and asymmetry of lower extremity in elderly women. *The Korean society of living environmental system*, 21(5), 672-680.
- Perry, J., & Burnfield, M. (2010). Gait analysis: Normal and pathological function. *Journal of sports science & medicine*, 9(2), 353.
- Plisky, P. J., Gorman, P. P., Butler, R. J., Kiesel, K. B., Underwood, F. B., & Elkins, B. (2009). The reliability of an instrumented device for measuring components of the star excursion balance test. *North American Journal of Sports Physical Therapy*, 4(2), 92-99.
- Pori, P., Kovčan, B., Vodičar, J., Dervišević, E., Karpljuk, D., Hadžić, V., & Šimenko, J. (2021). Predictive validity of the single leg hamstring bridge test in military settings. *Applied Sciences*, 11(4), 1822-1832.
- Robinson, R. O., Herzog, W., & Nigg, B. M. (1987). Use of force platform variables to quantify the effects of chiropractic manipulation on gait symmetry. *Journal of Manipulative and Physiological Therapeutics*, 10.
- Sadeghi, H., Allard, P., Prince, F., & Labelle, H. (2000). Symmetry and limb dominance in able-bodied gait: a review. *Gait & Posture*, 12(1), 34-45.
- Sakamoto, A. C. L., & Teixeira-Salmela, L. F., (2009). Muscular activation patterns during active prone hip extension exercises. *Journal of Electromyography and Kinesiology*, 19(1), 105-112.
- Shaikh, S. M., & Moharkar, A. C. (2020). Effect of core stability exercises versus Surya Namaskar on hamstring tightness in healthy adults using active knee extension test at the end of 6 weeks: A comparative study. *International Journal of Applied Research*, 6(3), 386-390.
- Sharma, V., & Kaur, J. (2017). Effect of core strengthening with pelvic proprioceptive neuromuscular facilitation on trunk, balance, gait, and function in chronic stroke. *Journal of exercise rehabilitation*, 13(2), 200-205.
- Sutherland, D. H. (2001). The evolution of clinical gait analysis part I: kinesiological EMG. *Gait & Posture*, 14(1), 61-70.
- Tsaklis, P., Malliaropoulos, N., Mendiguchia, J., Korakakis, V., Tsapralis, K., Pyne, D., & Malliaras, P. (2015). Muscle and intensity based hamstring exercise classification in elite female track and field athletes: implications for exercise selection during rehabilitation. *Journal of Sports Medicine*, 6, 209-217.
- Varela, A. R., Sallis, R., Rowlands, A. V., & Sallis J. F. (2021). Physical Inactivity and COVID-19: When Pandemics Collide. *Journal of Physical Activity and Health*, 18(10), 1159-1160.
- Yanagisawa, O., & Fukutani, A. (2020). Muscle recruitment pattern of the hamstring muscles in hip extension and knee flexion exercises. *Journal of human kinetics*, 72(1), 51-59.
- Zifchock, R. A., Davis, I., Higginson, J., & Royer, T. (2008). The symmetry angle: A novel, robust method of quantifying asymmetry. *Gait and Posture*, 27(4), 622-627.